

Journal of the American Statistical Association



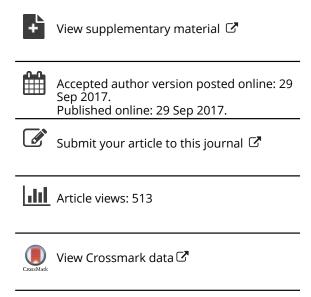
ISSN: 0162-1459 (Print) 1537-274X (Online) Journal homepage: https://www.tandfonline.com/loi/uasa20

Modeling Motor Learning Using Heteroscedastic Functional Principal Components Analysis

Daniel Backenroth, Jeff Goldsmith, Michelle D. Harran, Juan C. Cortes, John W. Krakauer & Tomoko Kitago

To cite this article: Daniel Backenroth, Jeff Goldsmith, Michelle D. Harran, Juan C. Cortes, John W. Krakauer & Tomoko Kitago (2018) Modeling Motor Learning Using Heteroscedastic Functional Principal Components Analysis, Journal of the American Statistical Association, 113:523, 1003-1015, DOI: 10.1080/01621459.2017.1379403

To link to this article: https://doi.org/10.1080/01621459.2017.1379403







Modeling Motor Learning Using Heteroscedastic Functional Principal Components Analysis

Daniel Backenroth^a, Jeff Goldsmith^a, Michelle D. Harran^{b,c}, Juan C. Cortes^{b,d}, John W. Krakauer^{b,c,d}, and Tomoko Kitago^{b,e}

^aDepartment of Biostatistics, Mailman School of Public Health, Columbia University, New York, NY; ^bDepartment of Neurology, Columbia University Medical Center, New York, NY; ^cDepartment of Neuroscience, Johns Hopkins University School of Medicine, Baltimore, MD; ^dDepartment of Neurology, Johns Hopkins University School of Medicine, Baltimore, MD; ^eBurke Neurological Institute, White Plains, NY

ABSTRACT

We propose a novel method for estimating population-level and subject-specific effects of covariates on the variability of functional data. We extend the functional principal components analysis framework by modeling the variance of principal component scores as a function of covariates and subject-specific random effects. In a setting where principal components are largely invariant across subjects and covariate values, modeling the variance of these scores provides a flexible and interpretable way to explore factors that affect the variability of functional data. Our work is motivated by a novel dataset from an experiment assessing upper extremity motor control, and quantifies the reduction in movement variability associated with skill learning. The proposed methods can be applied broadly to understand movement variability, in settings that include motor learning, impairment due to injury or disease, and recovery. Supplementary materials for this article are available online.

ARTICLE HISTORY

Received February 2016 Revised August 2017

KEYWORDS

Functional data; Kinematic data; Motor control; Probabilistic PCA; Variance modeling; Variational Bayes

1. Scientific Motivation

1.1. Motor Learning

Recent work in motor learning has suggested that change in movement variability is an important component of improvement in motor skill. It has been suggested that when a motor task is learned, variance is reduced along dimensions relevant to the successful accomplishment of the task, although it may increase in other dimensions (Scholz and Schöner 1999; Yarrow, Brown, and Krakauer 2009). Experimental work, moreover, has shown that learning-induced improvement of movement execution, measured through the trade-off between speed and accuracy, is accompanied by significant reductions in movement variability. In fact, these reductions in movement variability may be a more important feature of learning than changes in the average movement (Shmuelof, Krakauer, and Mazzoni 2012). These results have typically been based on assessments of variability at a few time points, for example, at the end of the movement, although high-frequency laboratory recordings of complete movements are often available.

In this article we develop a modeling framework that can be used to quantify movement variability based on dense recordings of fingertip position throughout movement execution. This framework can be used to explore many aspects of motor skill and learning: differences in baseline skill among healthy subjects, effects of repetition and training to modulate variability over time, or the effect of baseline stroke severity on movement

variance and recovery (Krakauer 2006). By taking full advantage of high-frequency laboratory recordings, we shift focus from particular time points to complete curves. Our approach allows us to model the variability of these curves as they depend on covariates, like the hand used or the repetition number, as well as the estimation of random effects reflecting differences in baseline variability and learning rates among subjects.

Section 1.2 describes our motivating data in more detail, and Section 2 introduces our modeling framework. A review of relevant statistical work appears in Section 3. Details of our estimation approach are in Section 4. Simulations and the application to our motivating data appear in Sections 5 and 6, respectively, and we close with a discussion in Section 7.

1.2. Dataset

Our motivating data were gathered as part of a study of motor learning among healthy subjects. Kinematic data were acquired in a standard task used to measure control of reaching movements. In this task, subjects rest their forearm on an air-sled system to reduce effects of friction and gravity. The subjects are presented with a screen showing eight targets arranged in a circle around a starting point, and they reach with their arm to a target and back when it is illuminated on the screen. Subjects' movements are displayed on the screen, and they are rewarded with 10 points if they turn their hand around within the target, and 3 or 1 otherwise, depending on how far their hand is from

the target at the point of return. Subjects are not rewarded for movements outside prespecified velocity thresholds.

Our dataset consists of 9481 movements by 26 right-handed subjects. After becoming familiarized with the experimental apparatus, each subject made 24 or 25 reaching movements to each of the 8 targets, in a semirandom order, with both the left and right hand. Movements that did not reach at least 30% of the distance to the target and movements with a direction more than 90 deg away from the target direction at the point of peak velocity were excluded from the dataset, because of the likelihood that they were made to the wrong target or not attempted due to distraction. Movements made at speeds outside the range of interest, with peak velocity less than 0.04 or greater than 2.0 m/s, were also excluded. These exclusion rules and other similar rules have been used previously in similar kinematic experiments, and are designed to increase the specificity of these experiments for probing motor control mechanisms (Huang et al. 2012; Tanaka, Sejnowski, and Krakauer 2009; Kitago et al. 2015). A small number of additional movements were removed from the dataset due to instrumentation and recording errors. The data we consider have not been previously reported.

For each movement, the X and Y position of the hand movement is recorded as a function of time from movement onset to the initiation of return to the starting point, resulting in bivariate functional observations denoted $[P_{ij}^X(t), P_{ij}^Y(t)]$ for subject i and movement j. In practice, observations are recorded not as functions but as discrete vectors. There is some variability in movement duration, which we remove for computational convenience by linearly registering each movement onto a common grid of length D=50. The structure of the registered kinematic data is illustrated in Figure 1. The top and bottom rows show, respectively, the first and last right-hand movement made to

each target by each subject. The reduction in movement variability after practice is clear.

Prior to our analyses, we rotate curves so that all movements extend to the target at 0° . This rotation preserves shape and scale, but improves interpretation. After rotation, movement along the X coordinate represents movement parallel to the line between origin and target, and movement along the Y coordinate represents movement perpendicular to this line. We build models for X and Y coordinate curves separately in our primary analysis. An alternative bivariate analysis appears in Appendix C.

2. Model for Trajectory Variability

We adopt a functional data approach to model position curves $P_{ij}(t)$. Here we omit the X and Y superscripts for notational simplicity. Our starting point is the functional principal component analysis (FPCA) model of Yao, Müller, and Wang (2005) with subject-specific means. In this model, it is assumed that each curve $P_{ij}(t)$ can be modeled as

$$P_{ij}(t) = \mu_{ij}(t) + \delta_{ij}(t)$$

$$= \mu_{ij}(t) + \sum_{k=1}^{\infty} \xi_{ijk} \phi_k(t) + \epsilon_{ij}(t). \tag{1}$$

Here $\mu_{ij}(t)$ is the mean function for curve $P_{ij}(t)$, the deviation $\delta_{ij}(t)$ is modeled as a linear combination of eigenfunctions $\phi_k(t)$, the ξ_{ijk} are uncorrelated random variables with mean 0 and variances λ_k , where $\sum_k \lambda_k < \infty$ and $\lambda_1 \geq \lambda_2 \geq \cdots$, and $\epsilon_{ij}(t)$ is white noise. Here all the deviations $\delta_{ij}(t)$ are assumed to have the same distribution, that of a single underlying random process $\delta(t)$.

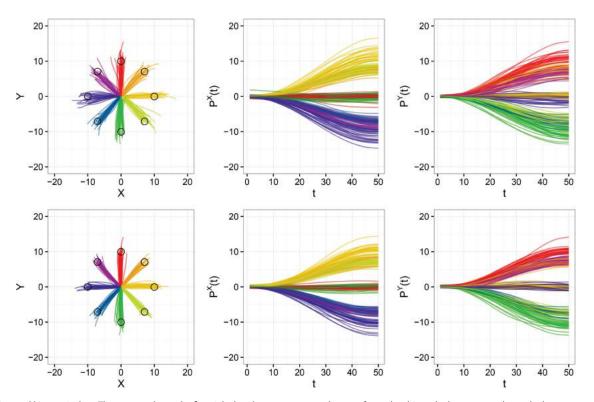


Figure 1. Observed kinematic data. The top row shows the first right-hand movement to each target for each subject; the bottom row shows the last movement. The left panel of each row shows observed reaching data in the X and Y plane. Targets are indicated with circles. The middle and right panels of each row show the $P_{ij}^X(t)$ and $P_{ij}^Y(t)$ curves, respectively.

Model (1) is based on a truncation of the Karhunen-Loève representation of the random process $\delta(t)$. The Karhunen-Loève representation, in turn, arises from the spectral decomposition of the covariance of the random process $\delta(t)$ from Mercer's Theorem, from which one can obtain eigenfunctions $\phi_k(t)$ and eigenvalues λ_k .

The assumption of constant score variances λ_k in model (1) is inconsistent with our motivating data because it implies that the variability of the position curves $P_{ij}(t)$ is not covariate- or subject-dependent. However, movement variability can depend on the subject's baseline motor control and may change in response to training. Indeed, these changes in movement variance are precisely our interest.

In contrast to the preceding, we therefore assume that each random process $\delta_{ij}(t)$ has a potentially unique distribution, with a covariance operator that can be decomposed as

$$\operatorname{cov}[\delta_{ij}(s), \delta_{ij}(t)] = \sum_{k=1}^{\infty} \lambda_{ijk} \phi_k(s) \phi_k(t),$$

so that the eigenvalues λ_{ijk} , but not the eigenfunctions, vary among the curves. We assume that deviations $\delta_{ij}(t)$ are uncorrelated across both i and j.

The model we pose for the $P_{ij}(t)$ is therefore

$$P_{ij}(t) = \mu_{ij}(t) + \sum_{k=1}^{K} \xi_{ijk} \phi_k(t) + \epsilon_{ij}(t),$$
 (2)

where we have truncated the expansion in model (1) to K eigenfunctions, and into which we incorporate covariate and subject-dependent heteroscedasticity with the score variance model

$$\lambda_{ijk} = \lambda_{k|\mathbf{x}_{ijk}^{*}, \mathbf{z}_{ijk}^{*}, \mathbf{g}_{ik}} = \operatorname{Var}(\xi_{ijk}|\mathbf{x}_{ijk}^{*}, \mathbf{z}_{ijk}^{*}, \mathbf{g}_{ik})$$

$$= \exp\left(\gamma_{0k} + \sum_{l=1}^{L^{*}} \gamma_{lk} \mathbf{x}_{ijlk}^{*} + \sum_{m=1}^{M^{*}} g_{imk} \mathbf{z}_{ijmk}^{*}\right)$$
(3)

where, as before, ξ_{ijk} is the kth score for the jth curve of the ith subject. In model (3), γ_{0k} is an intercept for the variance of the scores, γ_{lk} are fixed effects coefficients for covariates x_{ijlk}^* , $l=1,\ldots,L^*$, and g_{imk} are random effects coefficients for covariates z_{ijmk}^* , $m=1,\ldots,M^*$. The vector \mathbf{g}_{ik} consists of the concatenation of the coefficients g_{imk} , and likewise for the vectors \mathbf{x}_{ijk}^* and \mathbf{z}_{ijk}^* . Throughout, the subscript k indicates that models are used to describe the variance of scores associated with each basis function $\phi_k(t)$ separately. The covariates x_{ijlk}^* and z_{ijmk}^* in model (3) need not be the same across principal components. This model allows exploration of the dependence of movement variability on covariates, like progress through a training regimen, as well as of idiosyncratic subject-specific effects on variance through the incorporation of random intercepts and slopes.

Together, models (2) and (3) induce a subject- and covariate-dependent covariance structure for $\delta_{ij}(t)$:

$$\operatorname{cov}[\delta_{ij}(s), \delta_{ij}(t) | \boldsymbol{x}_{ijk}^*, \boldsymbol{z}_{ijk}^*, \boldsymbol{\phi}_k, \boldsymbol{g}_{ik}]$$

$$= \sum_{k=1}^K \lambda_{k|\boldsymbol{x}_{ijk}^*, \boldsymbol{z}_{ijk}^*, \boldsymbol{g}_{ik}} \phi_k(s) \phi_k(t).$$

In particular, the $\phi_k(t)$ are assumed to be eigenfunctions of a conditional covariance operator. Our proposal can be related to standard FPCA by considering covariate values random and marginalizing across the distribution of random effects and covariates using the law of total covariance:

$$\begin{aligned} \cos[\delta_{ij}(s), \delta_{ij}(t)] &= E\left\{\cos[\delta_{ij}(s), \delta_{ij}(t)|\boldsymbol{x}^*, \boldsymbol{z}^*, \boldsymbol{g}]\right\} \\ &+ \cos\left\{E[\delta_{ij}(s)|\boldsymbol{x}^*, \boldsymbol{z}^*, \boldsymbol{g}]E[\delta_{ij}(t)|\boldsymbol{x}^*, \boldsymbol{z}^*, \boldsymbol{g}]\right\} \\ &= \sum_{k=1}^K E\left[\lambda_{k|\boldsymbol{x}^*_{ijk}, \boldsymbol{z}^*_{ijk}, \boldsymbol{g}_{ik}}\right] \phi_k(s)\phi_k(t). \end{aligned}$$

We assume that the basis functions $\phi_k(t)$ do not depend on covariate or subject effects, and are therefore unchanged by this marginalization. Scores ξ_{ijk} are marginally uncorrelated over k; this follows from the assumption that scores are uncorrelated in our conditional specification, and holds even if random effects \mathbf{g}_{ik} are correlated over k. Finally, the order of marginal variances $E[\lambda_{k|\mathbf{x}_{ijk}^*, \mathbf{z}_{ijk}^*, \mathbf{g}_{ik}}]$ may not correspond to the order of conditional variances $\lambda_{k|\mathbf{x}_{ijk}^*, \mathbf{z}_{ijk}^*, \mathbf{g}_{ik}}$ for some or even all values of the covariates and random effects coefficients.

In our approach, we assume that the scores ξ_{ijk} have mean zero. For this assumption to be valid, the mean $\mu_{ij}(t)$ in model (2) should be carefully modeled. To this end we use the well-studied multilevel function-on-scalar regression model (Guo 2002; Di et al. 2009; Morris and Carroll 2006; Scheipl, Staicu, and Greven 2015),

$$\mu_{ij}(t) = \beta_0(t) + \sum_{l=1}^{L} x_{ijl} \beta_l(t) + \sum_{m=1}^{M} z_{ijm} b_{im}(t).$$
 (4)

Here $\beta_0(t)$ is the functional intercept; x_{ijl} for $l \in 1, ..., L$ are scalar covariates associated with functional fixed effects with respect to the curve $P_{ij}(t)$; $\beta_l(t)$ is the functional fixed effect associated with the lth such covariate; z_{ijm} for $m \in 1, ..., M$ are scalar covariates associated with functional random effects with respect to the curve $P_{ij}(t)$; and $b_{im}(t)$ for $m \in 1, ..., M$ are functional random effects associated with the ith subject.

Keeping the basis functions constant across all subjects and movements, as in conventional FPCA, maintains the interpretability of the basis functions as the major patterns of variation across curves. Moreover, the covariate and subject-dependent score variances reflect the proportion of variation attributable to those patterns. To examine the appropriateness of this assumption for our data, we estimated basis functions for various subsets of movements using a traditional FPCA approach, after rotating observed data so that all movements extend to the target at 0°. As illustrated in Figure 2, the basis functions for movements made by both hands and at different stages of training are similar.

3. Prior Work

FPCA has a long history in functional data analysis. It is commonly performed using a spectral decomposition of the sample covariance matrix of the observed functional data (Ramsay and Silverman 2005; Yao, Müller, and Wang 2005). Most relevant to our current work are probabilistic and Bayesian approaches based on nonfunctional PCA methods (Tipping and Bishop

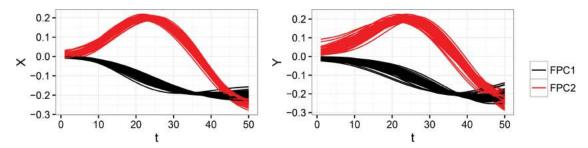


Figure 2. FPC basis functions estimated for various data subsets after rotating curves onto the positive X axis. The left panel shows the first and second FPC basis functions estimated for the X coordinate of movements to each target, for the left and right hand separately, and separately for movement numbers 1-6, 7-12, 13-18, and 19-24. The right panel shows the same for the Y coordinate.

1999; Bishop 1999; Peng and Paul 2009). Rather than proceeding in stages, first by estimating basis functions and then, given these, estimating scores, such approaches estimate all parameters in model (1) jointly. James, Hastie, and Sugar (2000) focused on sparsely observed functional data and estimated parameters using an EM algorithm; van der Linde (2008) took a variational Bayes approach to estimation of a similar model. Goldsmith, Zipunnikov, and Schrack (2015) considered both exponential-family functional data and multilevel curves, and estimated parameters using Hamiltonian Monte Carlo.

Some previous work has allowed for heteroskedasticity in FPCA. Chiou, Müller, and Wang (2003) developed a model which uses covariate-dependent scores to capture the covariate dependence of the mean of curves. In a manner that is constrained by the conditional mean structure of the curves, some covariate dependence of the variance of curves is also induced; the development of models for score variance was, however, not pursued. Here, by contrast, our interest is to use FPCA to model the effects of covariates on curve variance, independently of the mean structure. We are not using FPCA to model the mean; rather, the mean is modeled by the functionon-scalar regression model (4). Jiang and Wang (2010) introduce heteroscedasticity by allowing both the basis functions and the scores in an FPCA decomposition to depend on covariates. Briefly, rather than considering a bivariate covariance as the object to be decomposed, the authors pose a covariance surface that depends smoothly on a covariate. Aside from the challenge of incorporating more than a few covariates or subject-specific effects, it is difficult to use this model to explore the effects of covariates on heteroscedasticity: covariates affect both the basis functions and the scores, making the interpretation of scores and score variances at different covariate levels unclear. Although it does not allow for covariate-dependent heteroscedasticity, the model of Huang, Li, and Guan (2014) allows curves to belong to one of a few different clusters, each with its own FPCs and score variances.

In contrast to the existing literature, our model provides a general framework for understanding covariate and subject-dependent heteroskedasticity in FPCA. This allows the estimation of rich models with multiple covariates and random effects, while maintaining the familiar interpretation of basis functions, scores, and score variances.

Variational Bayes methods, which we use here to approximate Bayesian estimates of the parameters in models (2) and (3), are computationally efficient and typically yield accurate point estimates for model parameters, although they provide only an approximation to the complete posterior distribution and

inference may suffer as a result (Ormerod and Wand 2012; Jordan 2004; Jordan et al. 1999; Titterington 2004). These tools have previously been used in functional data analysis (van der Linde 2008; Goldsmith, Wand, and Crainiceanu 2011; McLean et al. 2013); in particular, Goldsmith and Kitago (2016) used variational Bayes methods in the estimation of model (4).

4. Methods

The main contribution of this article is the introduction of subject and covariate effects on score variances in model (3). Several estimation strategies can be used within this framework. Here we describe three possible approaches. Later, these will be compared in simulations.

4.1. Sequential Estimation

Models (2) and (3) can be fit sequentially in the following way. First, the mean $\mu_{ij}(t)$ in model (2) is estimated through function-on-scalar regression under a working independence assumption of the errors; we use the function pffr in the refund package (Goldsmith et al. 2016) in R. Next, the residuals from the function-on-scalar regression are modeled using standard FPCA approaches to obtain estimates of principal components and marginal score variances; given these quantities, scores themselves can be estimated (Yao, Müller, and Wang 2005). For this step we use the function fpca.sc, also in the refund package, which is among the available implementations. Next, we reestimate the mean $\mu_{ij}(t)$ in model (2) with function-on-scalar regression using pffr, although now, instead of assuming independence, we decompose the residuals using the principal components and score variances estimated in the previous step. We then reestimate principal components and scores using fpca.sc. The final step is to model the score variances given these score estimates. Assuming that the scores are normally distributed conditional on random effects and covariates, model (3) induces a generalized gamma linear mixed model for ξ_{ijk}^2 , the square of the scores, with log link, coefficients γ_{lk} and g_{imk} , and shape parameter equal to 1/2. We fit this model with the 1me4 package, separately with respect to the scores for each principal component, in order to obtain estimates of our parameters of interest in the score variance model (Bates et al. 2015).

The first two steps of this approach are consistent with the common strategy for FPCA, and we account for non-constant score variance through an additional modeling step. We anticipate that this sequential approach will work reasonably well in many cases, but note that it arises as a sequence of models that treat estimated quantities as fixed. First, one estimates the mean; then one treats the mean as fixed to estimate the principal components and the scores; finally, one treats the scores as fixed to estimate the score variance model. Overall performance may deteriorate by failing to incorporate uncertainty in estimates in each step, particularly in cases of sparsely observed curves or high measurement error variances (Goldsmith, Greven, and Crainiceanu 2013). Additionally, because scores are typically estimated in a mixed model framework, the use of *marginal* score variances in the FPCA step can negatively impact score estimation and the subsequent modeling of *conditional* score variances.

4.2. Bayesian Approach

4.2.1. Bayesian Model

Jointly estimating all parameters in models (2) and (3) in a Bayesian framework is an appealing alternative to the sequential estimation approach. We expect this to be less familiar to readers than the sequential approach, and therefore provide a more detailed description.

Our Bayesian specification of these models is formulated in matrix form to reflect the discrete nature of the observed data. In the following Θ is a known $D \times K_{\theta}$ matrix of K_{θ} spline basis functions evaluated on the shared grid of length D on which the curves are observed. We assume a normal distribution of the scores ξ_{ijk} conditional on random effects and covariates:

$$\mathbf{p}_{ij} = \sum_{l=0}^{L} x_{ijl} \mathbf{\Theta} \boldsymbol{\beta}_{l} + \sum_{m=1}^{M} z_{ijm} \mathbf{\Theta} \boldsymbol{b}_{im} + \sum_{k=1}^{K} \xi_{ijk} \mathbf{\Theta} \boldsymbol{\phi}_{k} + \epsilon_{ij}$$

$$\boldsymbol{\beta}_{l} \sim \text{MVN} \left[0, \sigma_{\boldsymbol{\beta}_{l}}^{2} \mathbf{Q}^{-1} \right]; \sigma_{\boldsymbol{\beta}_{l}}^{2} \sim \text{IG} \left[\alpha, \beta \right]$$

$$\boldsymbol{b}_{i} \sim \text{MVN} \left[0, \sigma_{\boldsymbol{b}}^{2} ((1 - \pi) \mathbf{Q} + \pi \mathbf{I})^{-1} \right]; \sigma_{\boldsymbol{b}}^{2} \sim \text{IG} \left[\alpha, \beta \right]$$

$$\boldsymbol{\phi}_{k} \sim \text{MVN} \left[0, \sigma_{\boldsymbol{\phi}_{k}}^{2} \mathbf{Q}^{-1} \right]; \sigma_{\boldsymbol{\phi}_{k}}^{2} \sim \text{IG} \left[\alpha, \beta \right]$$

$$\boldsymbol{\xi}_{ijk} \sim \text{N} \left[0, \exp \left(\sum_{l=0}^{L^{*}} \gamma_{lk} x_{ijlk}^{*} + \sum_{m=1}^{M^{*}} g_{imk} z_{ijmk}^{*} \right) \right]$$

$$\boldsymbol{\gamma}_{lk} \sim \text{N} \left[0, \sigma_{\gamma_{lk}}^{2} \right]$$

$$\boldsymbol{g}_{ik} \sim \text{MVN} \left[0, \boldsymbol{\Sigma}_{\boldsymbol{g}_{k}} \right]; \boldsymbol{\Sigma}_{\boldsymbol{g}_{k}} \sim \text{IW} \left[\boldsymbol{\Psi}_{k}, \nu \right]$$

$$\boldsymbol{\epsilon}_{ij} \sim \text{MVN} \left[0, \sigma^{2} \boldsymbol{I} \right]; \sigma^{2} \sim \text{IG} \left[\alpha, \beta \right].$$
(5)

In model (5), i = 1, ..., I refers to subjects, $j = 1, ..., J_i$ refers to movements within subjects, and k = 1, ..., K refers to principal components. We define the total number of functional observations $n = \sum_{i=1}^{I} J_i$. The column vectors \boldsymbol{p}_{ij} and $\boldsymbol{\epsilon}_{ij}$ are the $D \times 1$ observed functional outcome and independent error term, respectively, on the finite grid shared across subjects for the jth curve of the ith subject. The vectors $\boldsymbol{\beta}_{l}$, for l = 0, ..., L, are functional effect spline coefficient vectors, \boldsymbol{b}_{im} , for i = 1, ..., I and m = 1, ..., M, are random effect spline coefficient vectors, and $\boldsymbol{\phi}_k$, for k = 1 ..., K, are principal component spline coefficient vectors, all of length K_{θ} . \boldsymbol{Q} is a penalty matrix of the form $\boldsymbol{\Theta}^T \boldsymbol{M}^T \boldsymbol{M} \boldsymbol{\Theta}$, where \boldsymbol{M} is a matrix that penalizes the second derivative of the estimated functions. \boldsymbol{I} is the identity matrix. MVN refers to the multivariate normal distribution, N

to the normal distribution, IG to the inverse-gamma distribution, and IW to the inverse-Wishart distribution. Models (3) and (4) can be written in the form of model (5) above by introducing into those models covariates x_{ij0k}^* (in model (3), multiplying γ_{0k}) and γ_{0k} and γ_{0k} (in model (4), multiplying γ_{0k}), identically equal to 1. Some of the models used here, like in our real data analysis, do not have a global functional intercept γ_{0k} or global score variance intercepts γ_{0k} ; in these models there are no such covariates identically equal to 1.

As discussed further in Section 4.2.3, for purposes of identifiability and to obtain FPCs that represent non-overlapping directions of variation, when fitting this model we introduce the additional constraint that the FPCs should be orthonormal and that each FPC should explain the largest possible amount of variance in the data, conditionally on the previously estimated FPCs, if any.

In keeping with standard practice, we set the prior variances $\sigma_{\gamma lk}^2$ for the fixed-effect coefficients in the score variance model to a large constant, so that their prior is close to uniform. We set ν , the degrees of freedom parameter for the inverse-Wishart prior for the covariance matrices Σ_{g_k} , to the dimension of g_{ik} . We use an empirical Bayes approach, discussed further in Section 4.2.4, to specify Ψ_k , the scale matrix parameters of these inverse-Wishart priors. When the random effects g_{ik} are one-dimensional, this prior reduces to an inverse-Gamma prior. Sensitivity to prior specifications of this model should be explored, and we do so with respect to our real data analysis in Appendix D.

Variance components $\{\sigma_{\beta_l}^2\}_{l=0}^L$ and $\{\sigma_{\phi_k}^2\}_{k=1}^K$ act as tuning parameters controlling the smoothness of coefficient functions $\beta_l(t)$ and FPC functions $\phi_k(t)$, and our prior specification for them is related to standard techniques in semiparametric regression. σ_h^2 , meanwhile, is a tuning parameter that controls the amount of penalization of the random effects, and is shared across the $b_{im}(t)$, so that all random effects for all subjects share a common distribution. Whereas fixed effects and functional principal components are penalized only through their squared second derivative, the magnitude of the random effects is also penalized through the full-rank penalty matrix I to ensure identifiability (Scheipl, Staicu, and Greven 2015; Djeundje and Currie 2010). The parameter π , $0 < \pi < 1$, determines the balance of smoothness and shrinkage penalties in the estimation of the random effects $b_{im}(t)$. We discuss how to set the value of this parameter in Section 4.2.4. We set α and β , the parameters of the inverse-gamma prior distributions for the variance components, to 1.

Our framework can accommodate more complicated random effect structures. In our application in Section 6, for example, each subject has 8 random effect vectors \mathbf{g}_{ilk} , one for each target, indexed by $l=1,\ldots,8$; the index l is used here since in Section 6 l is used to index targets. We model the correlations between these random effect vectors through a nested random effect structure:

$$\mathbf{g}_{ilk} \sim \text{MVN}\left[\mathbf{g}_{ik}, \mathbf{\Sigma}_{\mathbf{g}_{ik}}\right]; \qquad \mathbf{g}_{ik} \sim \text{MVN}\left[0, \mathbf{\Sigma}_{\mathbf{g}_{k}}\right].$$
 (6)

Here the random effect vectors \mathbf{g}_{ilk} for subject i and FPC k, $l = 1, \dots 8$, are centered around a subject-specific random effect vector \mathbf{g}_{ik} . We estimate two separate random effect covariance

matrices, $\Sigma_{g_{ik}}$ and Σ_{g_k} , for each FPC k, one at the subjecttarget level and one at the subject level. These matrices are given inverse-Wishart priors, and are discussed further in Section 4.2.4.

4.2.2. Estimation Strategies

Sampling-based approaches to Bayesian inference of model (5) are challenging due to the constraints we impose on the $\phi_k(t)$ for purposes of interpretability of the score variance models, which are our primary interest. We present two methods for Bayesian estimation and inference for model (5): first, an iterative variational Bayes method, and second, a Hamiltonian Monte Carlo (HMC) sampler, implemented with the STAN Bayesian programming language (Stan Development Team 2013). Our iterative variational Bayes method, which estimates each parameter in turn conditional on currently estimated values of the other parameters, is described in detail in Appendix E. This appendix also includes a brief overview of variational Bayes methods. Our HMC sampler, also described in Appendix E, conditions on estimates of the FPCs and fixed and random functional effects from the variational Bayes method, and estimates the other quantities in model (5).

4.2.3. Orthonormalization

A well-known challenge for Bayesian and probabilistic approaches to FPCA is that the basis functions $\phi_k(t)$ are not constrained to be orthogonal. In addition, when the scores ξ_{iik} do not have unit variance, the basis functions will also be indeterminate up to magnitude, since any increase in their norm can be accommodated by decreased variance of the scores. Where interest lies in the variance of scores with respect to particular basis functions, it is important for the basis functions to be well-identified and orthogonal, so that they represent distinct and non-overlapping modes of variation. We therefore constrain estimated FPCs to be orthonormal and require each FPC to explain the largest possible amount of variance in the data, conditionally on the previously estimated FPCs, if any.

Let Ξ be the $n \times K$ matrix of principal component scores and ϕ the K by K_{θ} matrix of principal component spline coefficient vectors. In each step of our iterative variational Bayes algorithm, we apply the singular value decomposition to the matrix product $\mathbf{\Xi} \boldsymbol{\phi}^T \mathbf{\Theta}^T$; the orthonormalized principal component basis vectors which satisfy these constraints are then the right singular vectors of this decomposition. A similar approach was used to induce orthogonality of the principal components in the Monte Carlo Expectation Maximization algorithm of (Huang, Li, and Guan 2014) and as a post-processing step in (Goldsmith, Zipunnikov, and Schrack 2015). Although explicit orthonormality constraints may be possible in this setting (Šmídl and Quinn 2007), our simple approach, while not exact, provides for accurate estimation. Our HMC sampler conditions on the variational Bayes estimates of the FPCs, and therefore also satisfies the desired constraints.

4.2.4. Hyperparameter Selection

The parameter π in model (5) controls the balance of smoothness and shrinkage penalization in the estimation of the random effects b_{im} . In our variational Bayes approach we choose π to minimize the Bayesian information criterion (Schwarz 1978), following the approach of Djeundje and Currie (2010).

To set the hyperparameter Ψ_k in model (5) (or the hyperparameters in the inverse-Wishart priors for the variance parameters in model (6)), we use an empirical Bayes method. First, we estimate scores ξ_{ijk} using our variational Bayes method, with a constant score variance for each FPC. We then estimate the random effects g_{ik} (or g_{ilk}) using a generalized gamma linear mixed model, as described in Section 4.1. Finally, we compute the empirical covariance matrix corresponding to Σ_{g_k} (or $\Sigma_{g_{jk}}$ and Σ_{g_k}), and set the hyperparameter so that the mode of the prior distribution matches this empirical covariance matrix.

5. Simulations

We demonstrate the performance of our method using simulated data. Here we present a simulation that includes functional random effects as well as scalar score variance random effects. Appendix F includes additional simulations in a cross-sectional context which demonstrate the effect of varying the number of estimated FPCs, the number of spline basis functions, and the measurement error.

In our simulation design, the jth curve for the ith subject is generated from the model

$$P_{ij}(t) = 0 + b_i(t) + \sum_{k=1}^{4} \xi_{ijk} \phi_k(t) + \epsilon_{ij}(t).$$
 (7)

We observe the curves at D = 50 equally spaced points on the domain $[0, 2\pi]$. FPCs ϕ_1 and ϕ_2 correspond to the functions $\sin(x)$ and $\cos(x)$ and FPCs ϕ_3 and ϕ_4 correspond to the functions $\sin(2x)$ and $\cos(2x)$. We divide the curves equally into two groups m = 1, 2. We define x_{ij1}^* to be equal to 1 if the *i*th subject is assigned to group 1, and 0 otherwise, and we define x_{ij2}^* to be equal to 1 if the ith subject is assigned to group 2, and 0 otherwise. We generate scores ξ_{ijk} from zero-mean normal distributions with variances equal to

$$\operatorname{var}(\xi_{ijk}|\mathbf{x}_{ij}^*, g_{ik}) = \exp\left(\sum_{l=1}^2 \gamma_{lk} x_{ijl}^* + g_{ik}\right)$$
 (8)

We set γ_{1k} for k = 1, ..., 4 to the natural logarithms of 36, 12, 6 and 4, respectively, and γ_{2k} for $k = 1, \dots, 4$ to the natural logarithms of 18, 24, 12 and 6, respectively. The order of γ_{1k} and γ_{2k} for FPCs (represented by k) 1 and 2 black is purposely reversed between groups 1 and 2 so that the dominant mode of variation is not the same in the two groups. We generate the random effects g_{ik} in the score variance model from a normal distribution with mean zero and variance $\sigma_{g_k}^2$, setting $\sigma_{g_k}^2$ to 3.0, 1.0, 0.3, and 0.1 across FPCs. We simulate functional random effects $b_i(t)$ for each subject by generating 10 elements of a random effect spline coefficient vector from the distribution MVN[0, $\sigma_h^2((1-\pi)\mathbf{Q} + \pi \mathbf{I})^{-1}$], and then multiplying this vector by a B-spline basis function evaluation matrix. We set $\pi = \sigma_b^2 = 1/2000$, resulting in smooth random effects approximately one-third the magnitude of the FPC deviations. The $\epsilon_{ij}(t)$ are independent errors generated at all t from a normal distribution with mean zero and variance $\sigma^2 = 0.25$.

We fix the sample size I at 24, and set the number of curves per subject J_i to 4, 12, 24, and 48. Two hundred replicate datasets

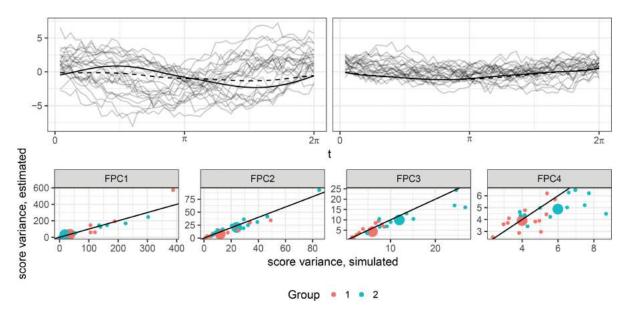


Figure 3. Selected results for the VB method for one simulation replicate with $I=J_i=24$. This simulation replicate was selected because the estimation quality of the group-level score variances, shown in the bottom row, is close to median with respect to all simulations. Panels in the top row show simulated curves for two subjects in light black, the simulated functional random effect for that subject as a dashed line, and the estimated functional random effect for that subject as a dark solid line. The subjects were selected to show one subject with a poorly estimated functional random effect (left) and one with a well estimated functional random effect (right). Panels in the bottom row show, for each FPC, estimates and simulated values of the group-level and subject-specific score variances. Large colored dots are the group-level score variances, and small colored dots are the estimated score variances for each subject, that is, they combine the fixed effect and the random effect.

were generated for each of the four scenarios. The simulation scenario with $I = J_i = 24$ is closest to the sample size in our real data application, where for each of 8 targets we have I = 26 and $I_i \approx 24$.

We fit the following model to each simulated dataset using each of the three approaches described in Section 4:

$$\mathbf{p}_{ij} = \mathbf{\Theta} \boldsymbol{\beta}_0 + \mathbf{\Theta} \boldsymbol{b}_i + \sum_{k=1}^4 \xi_{ijk} \mathbf{\Theta} \boldsymbol{\phi}_k + \boldsymbol{\epsilon}_{ij}$$
$$\xi_{ijk} \sim N \left[0, \exp \left(\sum_{l=1}^2 \gamma_{lk} x_{ijl}^* + g_{ik} \right) \right].$$

Here p_{ij} is the vectorized observation of $P_{ij}(t)$ from model (7). We use 10 spline basis functions for estimation, so that Θ is a 50×10 B-spline basis function evaluation matrix. For the Bayesian approaches, we use the priors specified in model (5), including N[0, 100] priors for variance parameters $\sigma_{\gamma lk}^2$. We use the empirical Bayes approach discussed in Section 4.2.4 to set the scale parameters for the inverse-gamma priors for the variances σ_{zk}^2 of the random effects g_{ik} .

ances $\sigma_{g_k}^2$ of the random effects g_{ik} .

Figures 3, 4, and 5 illustrate the quality of variational Bayes (VB) estimation of functional random effects, FPCs, and fixed and random effect score variance parameters. The top row of Figure 3 shows the collection of simulated curves for two

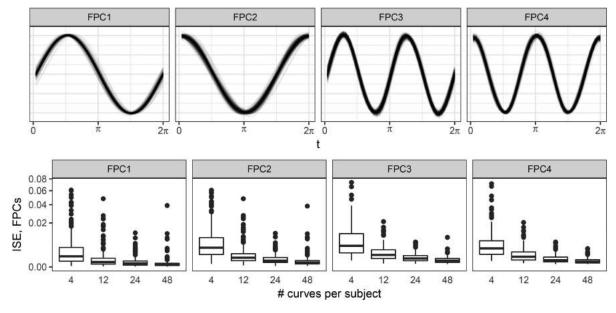


Figure 4. Estimation of FPCs using the VB method. Panels in the top row show a true FPC in dark black, and the VB estimates of that FPC for all simulation replicates with $J_i = 24$ in light black. Panels in the bottom row show, for each FPC and J_i , boxplots of integrated square errors (ISEs) for VB estimates $\widehat{\phi}_k(t)$ of each FPC $\phi_k(t)$, defined as ISE $= \int_0^{2\pi} [\phi_k(t) - \widehat{\phi}_k(t)]^2 dt$. The estimates in the top row therefore correspond to the ISEs for $J_i = 24$ shown in the bottom row. Figure A.10 in Appendix F shows examples of estimates of FPCs with a range of different ISEs.

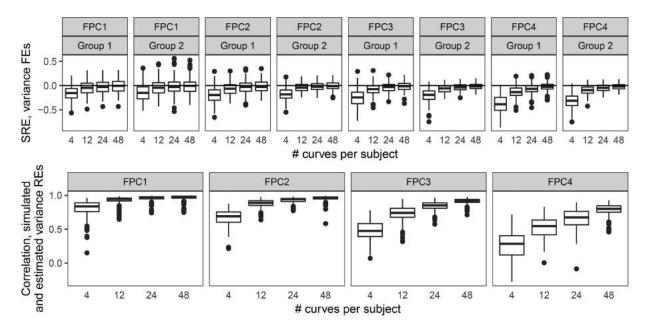


Figure 5. Estimation of score variance fixed and random effects using VB. Panels in the top row show, for each FPC, group, and J_i , boxplots of signed relative errors (SREs) for VB estimates $\widehat{\gamma_{lk}}$ of the fixed effect score variance parameters γ_{lk} , defined as SRE $=\frac{\widehat{\gamma_{lk}-\gamma_{lk}}}{\gamma_{lk}}$. Panels in the bottom row show, for each FPC and J_i , the correlation between random effect score variance parameters g_{ik} and their VB estimates. Intercepts and slopes for linear regressions of estimated on simulated random effect score variances are centered around 0 and 1, respectively (not shown).

subjects and includes the true and estimated subject-specific mean. The bottom row of this figure shows the true and estimated score variances across FPCs for a single simulated dataset, and suggests that fixed and random effects in the score variance model can be well-estimated.

The top row of Figure 4 shows estimated FPCs across all simulated datasets with $J_i = 24$; the FPCs are well-estimated and have no obvious systematic biases. The bottom row shows integrated squared errors (ISEs) for the FPCs across each possible J_i . As expected, the ISEs are smaller for the FPCs with larger score variances, and decrease as J_i increases. For 12 and especially for 4 curves per subject, estimates of the FPCs correspond to linear combinations of the simulated FPCs, leading to high ISEs and to inaccurate estimates of parameters in our score variance model (examples of poorly estimated FPCs can be seen in Appendix F).

Panels in the top row of Figure 5 show that estimates of fixed effect score variance parameters are shrunk towards zero, especially for lower numbers of curves per subject and FPCs 3 and 4. We attribute this to overfitting of the random effects in the mean model, which incorporates some of the variability attributable to the FPCs into the estimated random effects and reduces estimated score variances. Score variance random effects, shown in the bottom row of Figure 5, are more accurately estimated with more curves per subject.

Figure 6 and Table 1 show results from a comparison of the VB estimation procedure to the sequential estimation (SE) and Hamiltonian Monte Carlo (HMC) methods described in Section 4. We ran 4 HMC chains for 800 iterations each, and discarded the first 400 iterations from each chain. We assessed convergence of the chains by examining the convergence criterion of Gelman and Rubin (1992). Values of this criterion near 1 indicate convergence. For each of our simulation runs the criterion for every sampled variable was less than 1.1, and usually much closer to 1,

suggesting convergence of the chains. In general, performance for the VB and HMC methods is comparable, and both methods are in some respects superior to the performance of the SE method. Figure 6 compares the three methods' estimation of the score variance parameters. Especially for FPC 4, the SE method occasionally estimates random effect variances at 0; these are represented in the lower-right panel of Figure 6 as points where the correlation between simulated and estimated score variance random effects is 0. Table 1 shows, based on the simulation scenario with $J_i = 24$, the frequentist coverage of 95% credible intervals for the VB and HMC methods, and of 95% confidence intervals for the SE method, in each case, for the fixed effect score variance parameters γ_{lk} . For FPCs 3 and 4 especially, the SE procedure confidence intervals are too narrow. The median ISE for the functional random effects is about 30% higher with the VB method than with the SE method. This results from the relative tendency of the VB method to shrink FPC score estimates to zero; when the mean of the scores is in fact non-zero, this shifts estimated functional random effects away from zero. Other comparisons of these methods are broadly similar.

The HMC method is more computationally expensive than the other two methods. Running 4 chains for 800 iterations in parallel took approximately 90 minutes for $J_i = 24$. On one

Table 1. Coverage of 95% credible/confidence intervals for the score variance parameters γ_{lk} using the VB, SE, and HMC procedures, for $J_i=24$.

FPC	Group	VB	SE	НМС
1	1	0.955	0.915	0.960
1	2	0.945	0.905	0.945
2	1	0.940	0.935	0.940
2	2	0.980	0.935	0.975
3	1	0.965	0.930	0.975
3	2	0.955	0.885	0.980
4	1	0.930	0.775	0.970
4	2	0.940	0.705	0.965

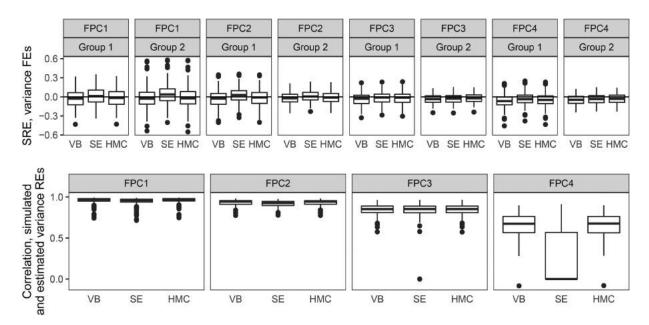


Figure 6. Comparison of estimation of score variance fixed and random effects using three methods. Panels in the top row show, for each FPC, group, and estimation method, boxplots of signed relative errors (SREs) for estimates of the fixed effect score variance parameters γ_{Ik} for $J_i = 24$. Panels in the bottom row show, for each FPC and estimation method, the correlation between random effect score variance parameters g_{ik} and their estimates for $J_i = 24$. Intercepts and slopes for linear regressions of estimated on simulated random effect score variances are centered around 0 and 1, respectively (not shown).

processor, by comparison, the SE method took about 20 minutes, almost entirely to run function-on-scalar regression using pffr. The VB method took approximately six minutes, including the grid search to set the value of the parameter π , which controls the balance between zeroth and second-derivative penalties in the estimation of functional random effects.

6. Analysis of Kinematic Data

We now apply the methods described above to our motivating dataset. To reiterate, our goal is to quantify the process of motor learning in healthy subjects, with a focus on the reduction of movement variability through repetition. Our dataset consists of 26 healthy, right-handed subjects making repeated movements to each of 8 targets. We focus on estimation, interpretation and inference for the parameters in a covariate and subject-dependent heteroscedastic FPCA model, with primary interest in the effect of repetition number in the model for score variance. We hypothesize that variance will be lower for later repetitions due to skill learning.

Prior to fitting the model, we rotate all movements to be in the direction of the target at 0° so that the X axis is the major axis of movement. For this reason, variation along the X axis is interpretable as variation in movement extent and variation along the Y axis is interpretable as variation in movement direction. We present results for univariate analyses of the $P_{ij}^X(t)$ and $P_{ij}^Y(t)$ position curves in the right hand and describe a bivariate approach to modeling the same data.

We present models with 2 FPCs, since 2 FPCs are sufficient to explain roughly 95% of the movement variability (and usually more) of movements remaining after accounting for fixed and random effects in the mean structure. Most of the variability of movements around the mean is explained by the first FPC, so we emphasize score variance of the first FPC as a convenient summary for the movement variability, and briefly present some results for the second FPC.

6.1. Model

We examine the effect of practice on the variability of movements while accounting for target and individual-specific idiosyncrasies. To do this, we use a model for score variance that includes a fixed intercept and slope parameter for each target and one random intercept and slope parameter for each subject-target combination. Correlation between score variance random effects for different targets for the same subject is induced via a nested random effects structure. The mean structure for observed curves consists of functional intercepts β_l for each target $l \in \{1, \ldots, 8\}$ and random effects b_{il} for each subject-target combination, to account for heterogeneity in the average movement across subjects and targets. Our heteroscedastic FPCA model is therefore:

$$\mathbf{p}_{ij} = \sum_{l=1}^{8} \mathbb{I}(\tan_{ij} = l) \left(\mathbf{\Theta} \boldsymbol{\beta}_{l} + \mathbf{\Theta} \boldsymbol{b}_{il} \right) + \sum_{k=1}^{K} \xi_{ijk} \mathbf{\Theta} \boldsymbol{\phi}_{k} + \boldsymbol{\epsilon}_{ij}$$
(9)

$$\xi_{ijk} \sim N \left[0, \sigma_{\xi_{ijk}}^2 = \exp\left(\sum_{l=1}^8 \mathbb{I}(tar_{ij} = l) \right) \right]$$

$$\left(\gamma_{lk,int} + g_{ilk,int} + (rep_{ij} - 1)(\gamma_{lk,slope} + g_{ilk,slope}) \right)$$

$$g_{ilk} \sim MVN \left[g_{ik}, \Sigma_{g_{ik}} \right]; g_{ik} \sim MVN \left[0, \Sigma_{g_k} \right]$$
(10)

The covariate tar_{ij} indicates the target to which movement j by subject i is directed. The covariate rep_{ij} indicates the repetition number of movement j, starting at 1, among all movements by subject i to the target to which movement j is directed, and $\mathbb{I}(\cdot)$ is the indicator function. To accommodate differences in baseline variance across targets, this model includes separate

population-level intercepts $\gamma_{lk,int}$ for each target l. The slopes $\gamma_{lk,slope}$ on repetition number indicate the change in variance due to practice for target *l*; negative values indicate a reduction in movement variance. To accommodate subject and targetspecific effects, each subject-target combination has a random intercept $g_{ilk,int}$ and a random slope $g_{ilk,slope}$, and each subject has an overall random intercept $g_{ik,int}$ and overall random slope gik, slope, in the score variance model for each functional principal component. This model parameterization allows different baseline variances and changes in variance for each target and subject, but shares FPC basis functions across targets. The model also assumes independence of functional random effects $b_{il}, l = 1, \dots, 8$ by the same subject to different targets, as well as independence of functional random effects b_{il} and score variance random effects \mathbf{g}_{ilk} for the same subject. The validity of these assumptions for our data are discussed in Appendix D.

Throughout, fixed effects $\gamma_{lk, \text{int}}$ and $\gamma_{lk, \text{slope}}$ are given N[0, 100] priors. Random effects $g_{ilk, \text{int}}$ and $g_{ilk, \text{slope}}$ are modeled using a bivariate normal distribution to allow for correlation between the random intercept and slope parameters in each FPC score variance model, and with nesting to allow for correlations between the random effects for the same subject and different targets. We use the empirical Bayes method described in Section 4.2.4 to set the scale matrix parameters of the inverse-Wishart priors for g_{ilk} and g_{ik} . Appendix D includes an analysis which examines the sensitivity of our results to various choices of prior hyperparameters.

We fit (9) and (10) using our VB method, with K=2 principal components and a cubic B-spline evaluation matrix Θ with $K_{\theta}=10$ basis functions.

6.2. Results

Figure 7 shows estimated score variances as a function of repetition number for *X* and *Y* coordinate right-hand movements to all targets. There is a decreasing trend in score variance for the first principal component scores for all targets and for both the *X* and *Y* coordinates, which agrees with our hypotheses regarding learning. Figure 7 also shows that nearly all of the variance of movement is attributable to the first FPC. Baseline variance is generally higher in the *X* direction than the *Y* direction, indicating that movement extent is generally more variable than movement direction.

To examine the adequacy of modeling score variance as a function of repetition number with a linear model, we compared the results of model (10) with a model for the score variances saturated in repetition number, i.e., where each repetition number m has its own set of parameters γ_{lkm} in the model for the score variances:

$$\xi_{ijk} \sim N \left[0, \sigma_{\xi_{ijk}}^2 = \exp\left(\sum_{l=1}^8 \sum_{m=1}^{24} \mathbb{I}(tar_{ij} = l, rep_{ij} = m) \gamma_{lkm} \right) \right].$$

$$\tag{11}$$

The results for these two models are included in Figure 7. The general agreement between the linear and saturated models suggests that the slope-intercept model is reasonable. For some targets score variance is especially high for the first movement,

which may reflect a familiarization with the experimental apparatus.

We now consider inference for the decreasing trend in variance for the first principal component scores. We are interested in the parameters $\gamma_{l1,slope}$, which estimate the population-level target-specific changes in score variance for the first principal component with each additional movement. Figure 8 shows VB estimates and 95% credible intervals for the $\gamma_{l1,slope}$ parameters for movements by the right hand to each target. All the point estimates $\gamma_{l1,slope}$ are lower than 0, indicating decreasing first principal component score variance with additional repetition. For some targets and coordinates there is substantial evidence that $\gamma_{l1,slope} < 0$; these results are consistent with our understanding of motor learning, although they do not adjust for multiple comparisons.

Appendix C includes results of a bivariate approach to modeling movement kinematics, which accounts for the 2-dimensional nature of the movement. In this approach, the *X* and *Y* coordinates of curves are concatenated, and each principal component reflects variation in both *X* and *Y* coordinates. For curves rotated to extend in the same direction, the results of this approach suggests that variation in movement extent (represented by the *X* coordinate) and movement direction (represented by the *Y* coordinate) are largely uncorrelated: the estimate of the first bivariate FPC represents variation primarily in the *X* coordinate, and is similar to the estimate of the first FPC in the *X* coordinate model, and vice versa for the second bivariate FPC. Analyses of score variance, then, closely follow the preceding univariate analyses.

Appendix B includes an analysis of data for one target using the VB, HMC, and SE methods. The three methods yield similar results.

7. Discussion

This article develops a framework for the analysis of covariate and subject-dependent patterns of movement variability in kinematic data. Our methods allow for flexible modeling of the covariate-dependence of variance of functional data with easily interpretable results. Our approach allows for the estimation of subject-specific effects on variance, as well as the consideration of multiple covariates. We are motivated by studies of motor control, and anticipate these methods can be broadly applied in this context; for example, ongoing work uses the methods developed here to study the initial post-stroke degree of impairment and the recovery process over time.

By applying these methods to our motivating dataset, we have demonstrated that movement variability is reduced with repetition. Results in Appendix A additionally show that the baseline level of skill of subjects is correlated across targets and hands, and that baseline movement variability is considerably greater in the non-dominant than the dominant hand. Further applications of these methods in scientifically important contexts could focus, for example, on whether movement variability is reduced with training faster in the dominant hand, or on whether training with one hand transfers skill to the other hand. Further research could also investigate target-specific differences in improvement of variance with training. Movements to some of the targets require coordination between the shoulder

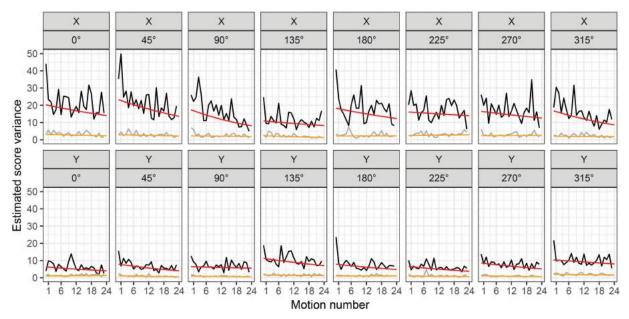


Figure 7. VB estimates of score variances for right hand movements to each target (in columns), separately for each direction (*X* or *Y*, in rows). Panels show the VB estimates of the score variance as a function of repetition number using the slope-intercept model (10) in red and orange (first and second FPC, respectively), and using the saturated one-parameter-per-repetition number model (11), in black and gray (first and second FPC, respectively).

and elbow, whereas others are primarily single-joint movements; the effectiveness of training may depend on the complexity of the movement.

We have provided three different estimation approaches for fitting heteroscedastic functional principal components models. Given its computational efficiency and comparable accuracy to the HMC and SE methods, we recommend use of the VB approach for exploratory analyses and model building. However, because of its approximate nature, we advise that any conclusions derived from the VB approach be confirmed with one of the other two methods, perhaps with a subset of the data if required for computational feasibility.

An alternative approach to the analysis of this dataset could treat the target effects $\gamma_{lk,\rm int}$ and $\gamma_{lk,\rm slope}$ in model (10) for the score variances as random effects centered around parameters $\mu_{k,\rm int}$ and $\mu_{k,\rm slope}$, representing the average across-target baseline score variance and change in score variance with repetition. Some advantages of this approach would be the

estimation of parameters that summarize the global effect of repetition on movement variability and shrinkage of the target-specific score variance parameters. However, with only 8 random target effects, the model would be sensitive to the specification of priors. Moreover, as discussed above, movements to different targets impose different demands on coordination and skill, which may reduce the interpretability of the parameters $\mu_{k,\mathrm{int}}$ and $\mu_{k,\mathrm{slope}}$.

Our analysis here is of curves linearly registered onto a common time domain, although our method could be applied to curves with different time domains, or to sparsely observed functional data. Our research group is currently working on developing an improved approach to registration in kinematic experiments which will take account of the repeated observations at the subject level by seeking to estimate subject-and curve-specific warping functions. This approach, combined with the methods we present in the current article, will eventually allow a more complete model for movement

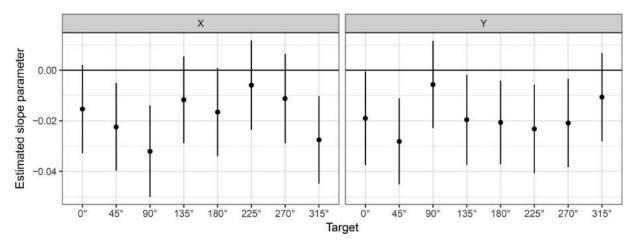


Figure 8. VB estimates of $\gamma_{\Pi, slope}$. This figure shows VB estimates and 95% credible intervals for target-specific score variance slope parameters $\gamma_{\Pi, slope}$ for movements by the right hand to each target, for the X and Y coordinates.



variability that takes into account both variability in movement duration and variability in movement trajectories.

There are several directions for further development. A full Bayesian treatment could estimate all quantities in model (5) jointly, or could condition on only the FPCs and jointly estimate all other quantities; given the very flexible nature of this model, additional constraints might be required in such a Bayesian treatment to improve identifiability. More complex models could allow for correlations between functional random effects and score variance random effects. Considering our data from the perspective of shape analysis may provide better understanding of interpretable movement features like location, scale and orientation (Kurtek et al. 2012; Gu, Pati, and Dunson 2012). Finally, an alternative approach to that presented here would be to model covariate-dependent score distributions through quantile regression. This may produce valuable insights into the complete distribution of movements, especially when this is not symmetric, but some work is needed to understand the connection of this technique to traditional FPCA.

8. Supplementary Materials

The supplementary materials contains the following appendices: A, containing additional results from our real data analysis; B, containing results comparing the VB, HMC and SE methods as applied to the kinematic data; C, containing a description of and results from a bivariate approach to the analysis of our kinematic data; D, containing a sensitivity analysis for our choice of hyperparameters and examining alternative mean specifications; E, containing a derivation of our variational Bayes algorithm and more detail on our HMC implementation; and F, containing additional simulation results.

The supplementary materials also include code implementing our methods and all the simulation scenarios presented here. This code can fit models in the form of model (5), provided that, as in our real data application and simulations, only one functional random effect is associated with each functional observation

Funding

The work of D. Backenroth and J. Goldsmith was supported in part by Award R21EB018917 from the National Institute of Biomedical Imaging and Bioengineering. The work of J. Goldsmith was also supported by Award R01NS097423-01 from the National Institute of Neurological Disorders and Stroke and Award R01HL123407 from the National Heart, Lung, and Blood Institute. National Heart, Lung, and Blood Institute [R01HL123407]; National Institute of Biomedical Imaging and Bioengineering [R21EB018917]; National Institute of Neurological Disorders and Stroke [R01NS097423-01].

References

- Bates, D., Mächler, M., Bolker, B., and Walker, S. (2015), "Fitting Linear Mixed-Effects Models Using lme4," *Journal of Statistical Software*, 67, 1–48. [1006]
- Bishop, C. M. (1999), "Bayesian PCA," Advances in Neural Information Processing Systems, 382–388. [1006]
- Chiou, J.-M., Müller, H.-G., and Wang, J.-L. (2003), "Functional Quasi-Likelihood Regression Models with Smooth Random Effects," *Journal* of the Royal Statistical Society, Series B, 65, 405–423. [1006]

- Di, C.-Z., Crainiceanu, C. M., Caffo, B. S., and Punjabi, N. M. (2009), "Multilevel Functional Principal Component Analysis," Annals of Applied Statistics, 4, 458–488. [1005]
- Djeundje, V. A. B., and Currie, I. D. (2010), "Appropriate Covariance-Specification via Penalties for Penalized Splines in Mixed Models for Longitudinal Data," *Electronic Journal of Statistics*, 4, 1202–1224. [1007,1008]
- Gelman, A., and Rubin, D. B. (1992), "Inference from Iterative Simulation Using Multiple Sequences," *Statistical Science*, 7, 457–472. [1010]
- Goldsmith, J., Greven, S., and Crainiceanu, C. M. (2013), "Corrected Confidence Bands for Functional Data using Principal Components," *Biometrics*, 69, 41–51. [1007]
- Goldsmith, J., and Kitago, T. (2016), "Assessing Systematic Effects of Stroke on Motor Control using Hierarchical Function-on-Scalar Regression," *Journal of the Royal Statistical Society*, Series C, 65, 215–236. [1006]
- Goldsmith, J., Scheipl, F., Huang, L., Wrobel, J., Gellar, J., Harezlak, J., McLean, M. W., Swihart, B., Xiao, L., Crainiceanu, C., and Reiss, P. T. (2016), refund: Regression with Functional Data. R package version 0.1-17, available at http://CRAN.R-project.org/package=refund [1006]
- Goldsmith, J., Wand, M. P., and Crainiceanu, C. M. (2011), "Functional Regression via Variational Bayes," *Electronic Journal of Statistics*, 5, 572-602. [1006]
- Goldsmith, J., Zipunnikov, V., and Schrack, J. (2015), "Generalized Multi-level Function-on-Scalar Regression and Principal Component Analysis," *Biometrics*, 71, 344–353. [1006,1008]
- Gu, K., Pati, D., and Dunson, D. B. (2012), "Bayesian Hierarchical Modeling of Simply Connected 2D Shapes," arXiv preprint arXiv:1201.1658.
 [1014]
- Guo, W. (2002), "Functional Mixed Effects Models," *Biometrics*, 58, 121–128. [1005]
- Huang, H., Li, Y., and Guan, Y. (2014), "Joint Modeling and Clustering Paired Generalized Longitudinal Trajectories with Application to Cocaine Abuse Treatment Data." Journal of the American Statistical Association, 83, 210–223. [1006,1008]
- Huang, V., Ryan, S., Kane, L., Huang, S., Berard, J., Kitago, T., Mazzoni, P., and Krakauer, J. (2012), "3D Robotic Training in Chronic Stroke Improves Motor Control but not Motor Function," Society for Neuroscience, October 2012, New Orleans. [1004]
- James, G. M., Hastie, T. J., and Sugar, C. A. (2000), "Principal Component Models for Sparse Functional Data," Biometrika, 87, 587–602. [1006]
- Jiang, C.-R., and Wang, J.-L. (2010), "Covariate Adjusted Functional Principal Components Analysis for Longitudinal Data," The Annals of Statistics, 38, 1194–1226. [1006]
- Jordan, M. I. (2004), "Graphical Models," Statistical Science, 19, 140–155. [1006]
- Jordan, M. I., Ghahramani, Z., Jaakkola, T. S., and Saul, L. K. (1999), "An Introduction to Variational Methods for Graphical Models," *Machine Learning*, 37, 183–233. [1006]
- Kitago, T., Goldsmith, J., Harran, M., Kane, L., Berard, J., Huang, S., Ryan, S. L., Mazzoni, P., Krakauer, J. W., and Huang, V. S. (2015), "Robotic Therapy for Chronic Stroke: General Recovery of Impairment or Improved Task-Specific Skill?" *Journal of Neurophysiology*, 114, 1885–1894. [1004]
- Krakauer, J. W. (2006), "Motor Learning: Its Relevance to Stroke Recovery and Neurorehabilitation," Current Opinion in Neurology, 19, 84–90.
 [1003]
- Kurtek, S., Srivastava, A., Klassen, E., and Ding, Z. (2012), "Statistical Modeling of Curves Using Shapes and Related Features," *Journal of the American Statistical Association*, 107, 1152–1165. [1014]
- McLean, M. W., Scheipl, F., Hooker, G., Greven, S., and Ruppert, D. (2013), "Bayesian Functional Generalized Additive Models for Sparsely Observed Covariates," under review. [1006]
- Morris, J. S. and Carroll, R. J. (2006), "Wavelet-Based Functional Mixed Models," *Journal of the Royal Statistical Society*, Series B, 68, 179–199. [1005]
- Ormerod, J., and Wand, M. P. (2012), "Gaussian Variational Approximation Inference for Generalized Linear Mixed Models," *The American Statistician*, 21, 2–17. [1006]
- Peng, J., and Paul, D. (2009), "A Geometric Approach to Maximum Likelihood Estimation of the Functional Principal Components from Sparse

- Longitudinal Data," *Journal of Computational and Graphical Statistics*, 18, 995–1015. [1006]
- Ramsay, J. O., and Silverman, B. W. (2005), Functional Data Analysis, New York: Springer. [1005]
- Scheipl, F., Staicu, A.-M., and Greven, S. (2015), "Functional Additive Mixed Models," *Journal of Computational and Graphical Statistics*, 24, 477–501. [1005,1007]
- Scholz, J.-P., and Schöner, G. (1999), "The Uncontrolled Manifold Concept: Identifying Control Variables for a Functional Task," *Experimental Brain Research*, 126, 289–306. [1003]
- Schwarz, G. (1978), "Estimating the Dimension of a Model," *The Annals of Statistics*, 6, 461–464. [1008]
- Shmuelof, L., Krakauer, J. W., and Mazzoni, P. (2012), "How is a Motor Skill Learned? Change and Invariance at the Levels of Task Success and Trajectory Control," *Journal of Neurophysiology*, 108, 578–594. [1003]
- Stan Development Team (2013), Stan Modeling Language User's Guide and Reference Manual, Version 1.3, available at http://mc-stan.org/ [1008]
- Tanaka, H., Sejnowski, T. J., and Krakauer, J. W. (2009), "Adaptation to Visuomotor Rotation Through Interaction between Posterior Parietal

- and Motor Cortical Areas," *Journal of Neurophysiology*, 102, 2921–2932. [1004]
- Tipping, M. E., and Bishop, C. (1999), "Probabilistic Principal Component Analysis," *Journal of the Royal Statistical Society*, Series B, 61, 611–622. [1006]
- Titterington, D. M. (2004), "Bayesian Methods for Neural Networks and Related Models," *Statistical Science*, 19, 128–139. [1006]
- van der Linde, A. (2008), "Variational Bayesian Functional PCA," Computational Statistics and Data Analysis, 53, 517–533. [1006]
- Šmídl, V., and Quinn, A. (2007), "On Bayesian Principal Component Analysis," Computational Statistics & Data Analysis, 51, 4101–4123.
- Yao, F., Müller, H., and Wang, J. (2005), "Functional Data Analysis for Sparse Longitudinal Data," *Journal of the American Statistical Associ*ation, 100, 577–590. [1004,1005,1006]
- Yarrow, L., Brown, P., and Krakauer, J.-W. (2009), "Inside the Brain of an Elite Athlete: The Neural Processes that Support High Achievement in Sports," *Nature Reviews Neuroscience*, 10, 585–596. [1003]